



Moner: Motion Correction in Undersampled Radial MRI with Unsupervised Neural Representation

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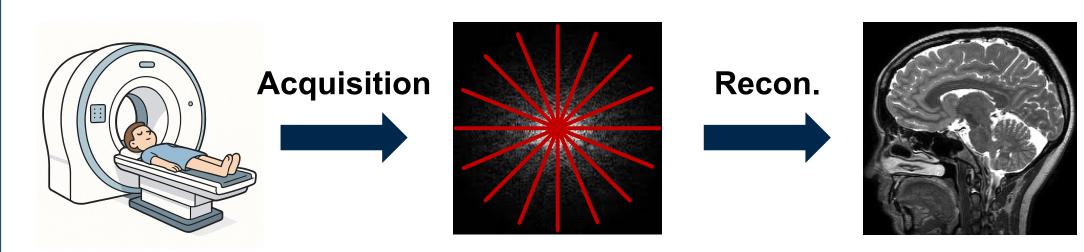


Overview

- Goal: Reconstruct motion-free MR images from rigid motion-corrupted k-data without using external data.
- Solution: Jointly estimate motion and images by integrating a quasi-static motion model into neural representation.
- Results: Our unsupervised approach outperforms SOTA supervised techniques on in- & out-of-domain data.

Background

- Radial Magnetic Resonance Imaging (MRI)
 - A medical imaging technique to image human anatomy.

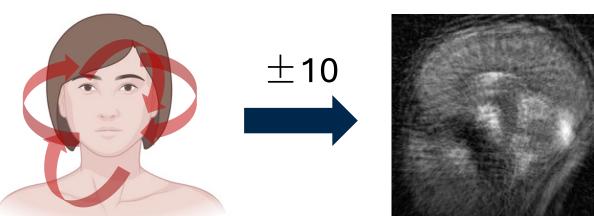


MRI scanner

k-data in Fourier space

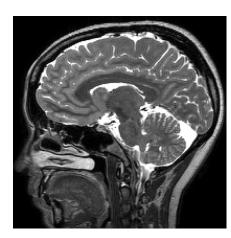
MR image

- Why is Motion Correction (MoCo) necessary in MRI?
 - Subject inevitably moves due to long scanning duration, which leads to severe motion artifacts in MR images.





Motion artifacts

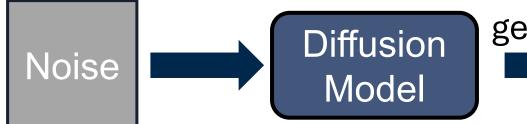


Motion-free

- The SOTA framework for MRI MoCo
- Combines MRI forward model (i.e., Fourier transform), a rigid motion model, and pre-trained neural networks.
- Jointly estimates motion and reconstructs MR images.

$$rg\min_{m{f},\,artheta,\,m{ au}}\sum_{orall(m{ heta},\omega)}\left\|\mathcal{T}_{\! heta,\omega}\{m{ ilde{f}}\,\}-m{k}(heta,\omega)
ight\|_2^2,\;\; ext{with}\;\;m{ ilde{f}}\,=\mathcal{R}(m{f};artheta,m{ au})$$

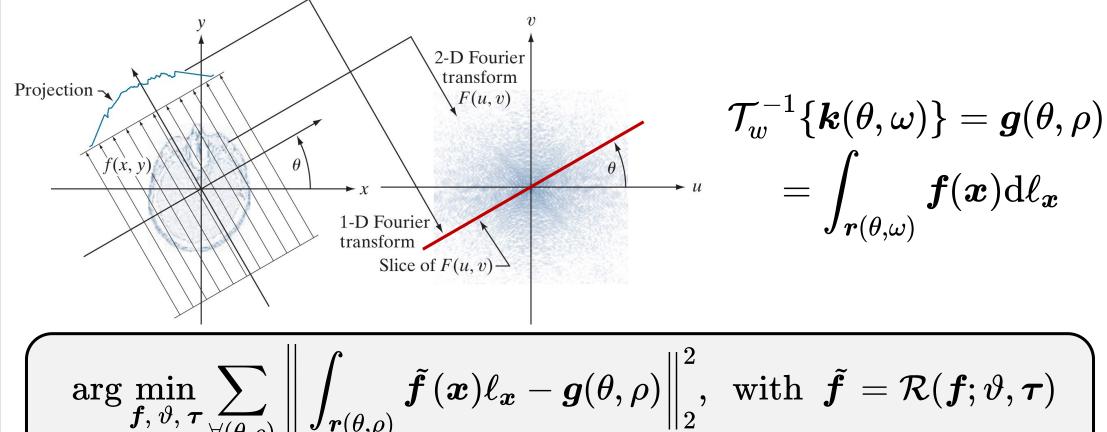
Score-MoCo using pre-trained diffusion model is SOTA.



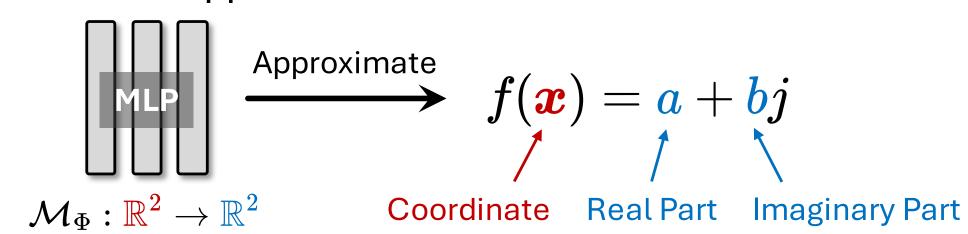


Our Solution

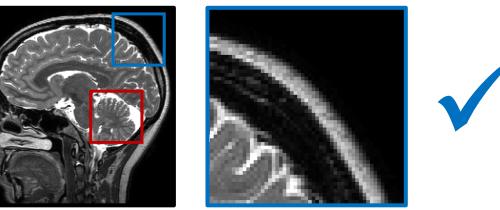
• Formulation: Reformulating radial MRI reconstruction as a back-projection problem via the Fourier-slice theorem.



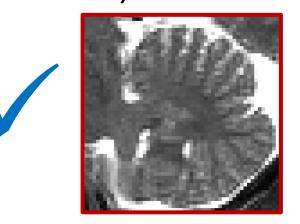
 Neural Representation: Using a coordinate-based neural network to approximate a continuous function of MR images.



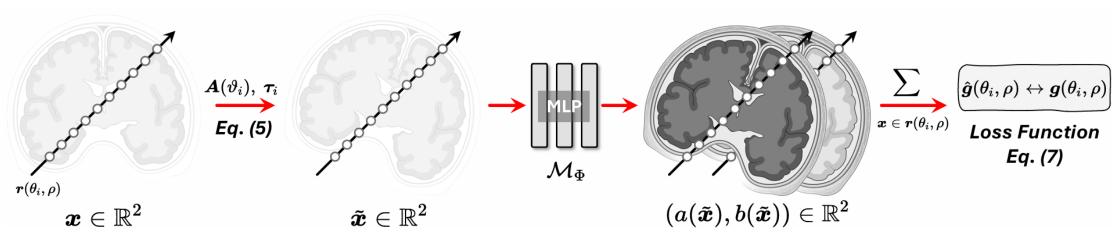
 Coarse-to-fine Image Recovery: Motion estimation mainly relies on low-frequency structures (e.g., skull), rather than high-frequency details (e.g., cerebellum).







Joint Motion Correction and MRI Reconstruction

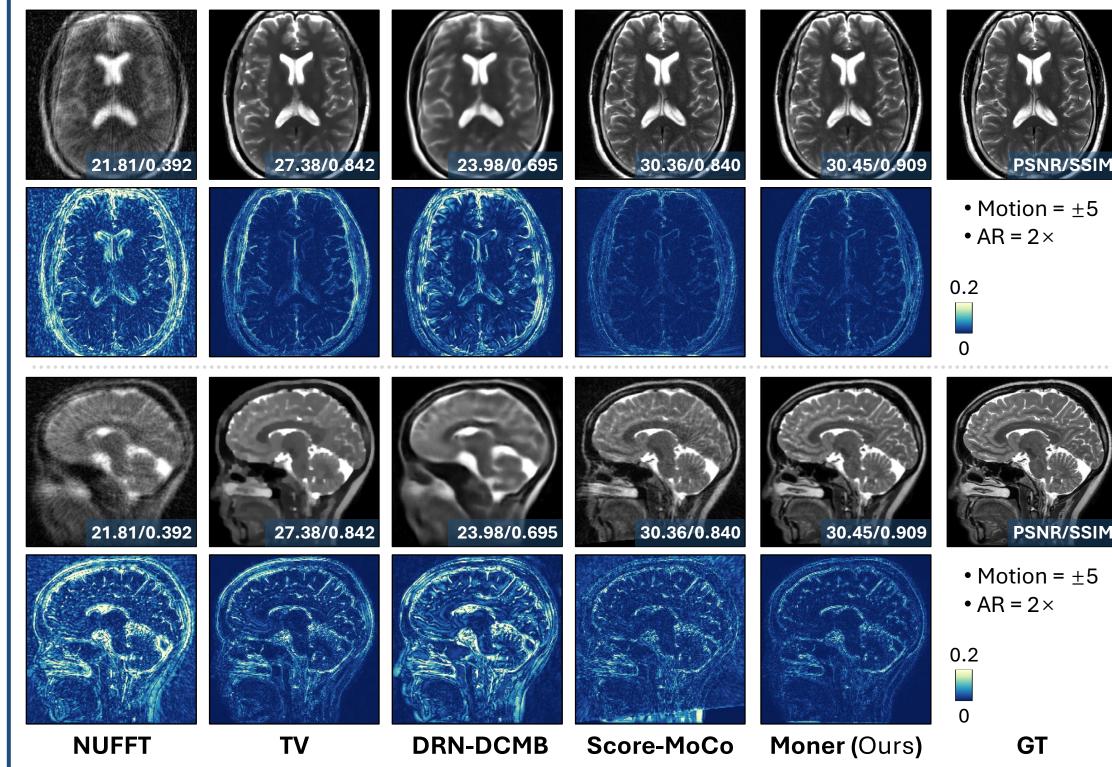


Four Steps:

- Sample multiple coordinates along ray paths in the canonical space.
- Transform sampled points to physical space using the motion model.
- Feed the transformed coordinates into the MLP to predict the MR image.
- Generate projection data via a differentiable projection model.
- Optimize MLP and motion parameters minimizing errors on projection data.

Experimental Results

Results on simulated 2D fastMRI and MoDL datasets



Results on an in-vivo 3D sample (scanning time ≈ 8 min.)

